طراحی، آنالیز و شبیه سازی حسگر زیست پزشکی ریز حلقه برای ایه بلور نوری

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چکیده - این مقاله به طراحی حسگرهای زیستی بر اساس ریزحلقه‌های بلور نوری می‌پردازد. ملکول‌های زیستی ضرایب شکست منحصر به فرد کود را دارند؛ بنابراین مشخصه‌های حسگر (خروجی، ضریب کیفیت و طول موج نوسان) برای هر کدام از ملکول‌های مختلفی متغیر و خاص خواهد داشت. یک ساختمان منفی با این مقاله مورد بررسی قرار داده شده و می‌تواند این ها انتخاب گردد.

کلید واژه: حسگر، بلور نوری، ضریب شکست، طول موج نوسان، سیستم‌های میکرو‌الکترو مکانیکی

Design, analysis and simulation of a Ring Resonator Based bioMEMS sensor by using a photonic crystal

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Abstract- This paper presents the design of a photonic crystal ring resonator based bio MEMS sensor to detect divergent biochemical molecules. As the biochemical molecules have exclusive refractive indices, the resonant wavelength, output transmission and other parameters are varied from one chemical to the other. Two different structures are surveyed to choose the best one.

Keywords: sensor; Photonic crystal; refractive index; resonant wavelength; MEMS

1. Introduction

This MEMS technology is used to produce this device because of its small size (they are less than 1 µm). The photonic crystals bioMEMS sensors have different usages in medical fields in recent decade. They are divided into various groups: ring resonators [1,2,3], plasmonic metamaterials [4,5,6], and waveguides [7]. These sensors are able to detect DNA, protein, antigen antibody interaction, cells and Bacteria [8,9].

Photonic Crystals are periodic structures which consist of different rods with different diameter and materials. They consist of periodic dielectric nanostructures. If electromagnetic waves pass through these crystals, their propagation is varied due to greater refractive index of these rods compared to that of air [1]. The motion of photons, which is affected by lattice properties, helps to detect and identify molecules easily. Thanks to these special properties, there is a band gap which does not let special wavelength pass [1]. However, it is possible to manipulate the wave propagation through PC by using defects in the structure.

In this paper, a photonic crystal ring resonator (PCRR) sensor is designed and analysed to detect different chemical and biochemical molecules. The design steps and simulation results are established.

2. Theory

PBG wavelengths cannot propagate through the PC; then, adding some defects into the structure manipulates the propagation. The sensor comprises of a ring resonator in a way that line defect performs as waveguides and the circular one is the ring. Changing the refractive index of the background causes a change in the resonant wavelength and output transmission. The Maxwell’s electromagnetic equation withdraws the sensor’s function.

The equation (1) demonstrate the sensing performance of the PC.

\[ L_{eff} = Q \lambda / (2 \pi \eta) \]  

\( Q \) is the resonator quality factor, \( \lambda \) is the resonant wavelength, and \( \eta \) is the refractive index of ring resonator. And \( L \) is the effective interaction length.

3. Designe

Both of sensors are fabricated by two dimensional photonic crystal ring resonator based on silicon rods in an air background. parameters of them are given in the table 1. The size of these structures is 9.45 µm * 9.45 µm. they involve 15 rods in length and 15 in width. The sensors are demonstrated in fig.1.

<table>
<thead>
<tr>
<th>features</th>
<th>amount</th>
</tr>
</thead>
<tbody>
<tr>
<td>The lattice constant (a)</td>
<td>0.63 um</td>
</tr>
<tr>
<td>Refractive index of Silicon rod’s</td>
<td>3.42</td>
</tr>
<tr>
<td>Refractive index of air</td>
<td>1</td>
</tr>
<tr>
<td>Radius of Rod (r)</td>
<td>0.132 um</td>
</tr>
</tbody>
</table>

Fig. 1: schematic of the proposed bio MEMS sensor: (a) parallel straight waveguides, (b) Cross straight waveguides

the first structure consists of two parallel straight waveguides. The other one consists of two Cross straight waveguides. The QF, resonance wavelength and transmission of first sensor are 445.6, 1.544 µm and 0.4. The QF, resonance
wavelength and transmission of second sensor are 525.19, 1.97 µm and 0.4.

The band structure diagram of these structures are the same and demonstrated in fig. 2. In this figure, the vertical axial is the normalized frequency. The band diagram consists of two PBG modes (TM and TE). There are two wavelength range for TE range. Moreover, from the fig. 2, there are two wavelengths for TM range, too. TE mode which is ranged from 2.51Hz to 4.35 Hz is chosen.

Fig. 2 band structure diagram of both structures.

4. Simulation results and discussion

Fig. 5 shows the normalized transmission spectrum to wavelength for first and second structures. Furthermore, Table 3 demonstrates the same parameters of second sensor for unlike molecules. The distinct refractive index of various molecules consequences in diverse transmission output and resonance wavelength volume. This information shows that which structure is able to sense the molecules.

From the above tables, it is obvious that the second PC based sensor has better properties. As it is seen, the QF has really low and unacceptable amount when the wave guides are parallel. However, the cross wave guides sensors show better amount of QF and transmission output. In addition, the sensitivity of parallel straight waveguides is 1300 nm/RIU, and the sensitivity of cross straight waveguide is 9250 nm/RIU. In comparison with parallel straight waveguides sensor, cross straight waveguide sensor shows better properties.

![Normalized Transmission Spectrum](image)

(a) Normalized transmission spectrum of the parallel straight waveguides sensor (b) Normalized transmission spectrum of the cross straight waveguide sensor

<table>
<thead>
<tr>
<th>Name of molecular</th>
<th>Refractive index</th>
<th>Resonant wavelength (um)</th>
<th>Q factor</th>
<th>Output transmission</th>
<th>references</th>
</tr>
</thead>
<tbody>
<tr>
<td>water</td>
<td>1.333</td>
<td>1.947</td>
<td>104.1</td>
<td>0.78</td>
<td>[10]</td>
</tr>
<tr>
<td>RK3E-ras</td>
<td>1.443</td>
<td>1.947</td>
<td>101.9</td>
<td>0.78</td>
<td>[11]</td>
</tr>
<tr>
<td>YD-10B</td>
<td>1.549</td>
<td>1.945</td>
<td>100.2</td>
<td>0.75</td>
<td>[11]</td>
</tr>
<tr>
<td>Cytosol</td>
<td>1.57</td>
<td>1.945</td>
<td>99.5</td>
<td>0.76</td>
<td>[12]</td>
</tr>
<tr>
<td>Nucleus</td>
<td>1.503</td>
<td>1.958</td>
<td>99.1</td>
<td>0.76</td>
<td>[12]</td>
</tr>
<tr>
<td>Blood Plasma</td>
<td>1.503</td>
<td>1.952</td>
<td>99.1</td>
<td>0.76</td>
<td>[11]</td>
</tr>
</tbody>
</table>

Table 2 refractive index, resonant wavelength, Q factor and transmission output of first sensor for different molecules.

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Table 3 refractive index, resonant wavelength, Q factor and transmission output of second sensor for different molecules.

<table>
<thead>
<tr>
<th>Name of molecular</th>
<th>Refractive index</th>
<th>Resonant wavelength (um)</th>
<th>Q factor</th>
<th>Output transmission</th>
<th>references</th>
</tr>
</thead>
<tbody>
<tr>
<td>water</td>
<td>1.333</td>
<td>2.32</td>
<td>300.5</td>
<td>0.82</td>
<td>[10]</td>
</tr>
<tr>
<td>RK3E-ras</td>
<td>1.373</td>
<td>2.25</td>
<td>202.09</td>
<td>0.74</td>
<td>[11]</td>
</tr>
<tr>
<td>YD-10B</td>
<td>1.369</td>
<td>2.41</td>
<td>237.9</td>
<td>0.34</td>
<td>[11]</td>
</tr>
<tr>
<td>Cytosol</td>
<td>1.360</td>
<td>2.08</td>
<td>297</td>
<td>0.85</td>
<td>[12]</td>
</tr>
<tr>
<td>Nucleus</td>
<td>1.355</td>
<td>2.04</td>
<td>379.3</td>
<td>0.58</td>
<td>[12]</td>
</tr>
<tr>
<td>Blood Plasma</td>
<td>1.350</td>
<td>2.04</td>
<td>373</td>
<td>0.7</td>
<td>[1]</td>
</tr>
</tbody>
</table>

6. Conclusions

In this paper, the sensors, consisting of two dimensional PC ring resonator with the cubic lattice of circular rod in air, was designed to detect different molecules. Numerical method was used to analyse the functional characteristics of these sensors. In addition, the different parameters of the sensor were measured, which showed significant differences in transmission output amplitude and resonant wavelength. In comparison with parallel straight waveguide sensor, cross straight waveguide sensor presented better QF. The sensor simplifies the detection of different molecules, assisting earlier finding of health problems.

References


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